

Evaluation of the Deconvolved Diffusion Spectrum Imaging Technique

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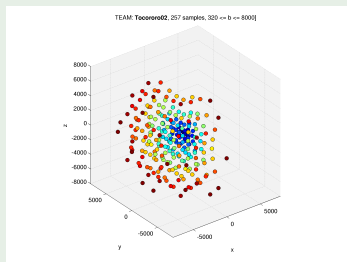
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- Description of the Reconstruction Method
- Example

Sampling scheme

Details

- $N = 257$ points in one hemisphere (volume).



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- The signal was duplicated on the other hemisphere to obtain 515 points [Wedeen V.J. et al., 2005].

References



Wedeen V.J. et al. Mapping complex tissue architecture with diffusion spectrum magnetic resonance imaging. *Magn Reson Med.*, 54(6), 1377-1386 (2005).

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- The signal was duplicated on the other hemisphere to obtain 515 points [Wedeen V.J. et al., 2005].
- $320 \leq \text{b-value} \leq 8000 \quad s/mm^2$
- Two datasets: isolated voxels (IV) and structured field (SF).
 $SNR = 5, 10, 15, 20, 25, 30, 35$ and 40 .
(<http://hardi.epfl.ch/contest.html>)

References



Wedeen V.J. et al. Mapping complex tissue architecture with diffusion spectrum magnetic resonance imaging. *Magn Reson Med.*, 54(6), 1377-1386 (2005).

Description of the Reconstruction Method

Pipeline

- 1 Conventional DSI Reconstruction
- 2 Deconvolved DSI
- 3 *ODF* Computation
- 4 *ODF* Maxima Extraction

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Conventional DSI Reconstruction

Description of the Reconstruction Method

Diffusion Spectrum Imaging (DSI)

$$P(r_x, r_y, r_z) = \iiint_{V=\{-\infty, \infty\}} E(q_x, q_y, q_z) e^{-2\pi i(r_x q_x + r_y q_y + r_z q_z)} dq_x dq_y dq_z,$$

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Diffusion Propagator

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Signal

where $[r_x, r_y, r_z]$ and $[q_x, q_y, q_z]$ are the Cartesian real- and q-space vectors.

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$$ODF(\hat{\mathbf{r}}) = \int_0^\infty P(\rho, \hat{\mathbf{r}}) \rho^2 d\rho, \quad \Rightarrow \text{Orientational Distribution Function}$$

where $[r_x, r_y, r_z] = \vec{r} = \rho \hat{\mathbf{r}}$ (Spherical coordinates).

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References



Wedeen V.J. et al. Mapping complex tissue architecture with diffusion spectrum magnetic resonance imaging. *Magn Reson Med.*, 54(6), 13771386 (2005).

Deconvolved DSI

Description of the Reconstruction Method

Theory

In practice: $\tilde{P} \approx \text{FastFourierTransform}(E)$

$$\tilde{P}(r_x, r_y, r_z) = \iiint_{V=\{-\infty, \infty\}} \square(q_x, q_y, q_z) E(q_x, q_y, q_z) e^{-2\pi i(r_x q_x + r_y q_y + r_z q_z)} dq_x dq_y dq_z,$$

where, $\square(q_x, q_y, q_z) = \begin{cases} 1 & \text{if } \sqrt{q_x^2 + q_y^2 + q_z^2} \leq q_{max}, \\ 0 & \text{otherwise.} \end{cases}$ (if $q_{max} = 5, 515$ points in $11 \times 11 \times 11$ grid)

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Convolution Theorem:

$\mathcal{F}(gk) = \mathcal{F}(g) \otimes \mathcal{F}(k)$, where $\mathcal{F}()$ denotes the Fourier Transform
and \otimes is the convolution operator.

Deconvolved DSI

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In practice: $\tilde{P} \approx \text{FastFourierTransform}(E)$

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$\mathcal{F}(\Pi) \implies$ Point Spread Function (PSF) of the experiment.

References



Canales-Rodríguez E.J. et al. Deconvolution in diffusion spectrum imaging. *Neuroimage*, 50(1), 136-49 (2010)

Deconvolved DSI

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deconvolution operator

Deconvolved DSI

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deconvolution operator

The deconvolution process was performed using the accelerated Lucy-Richardson algorithm [Biggs and Andrews, 1997].

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The deconvolution process was performed using the accelerated Lucy-Richardson algorithm [Biggs and Andrews, 1997].

- 1 This method conserves the constraints on frequency distributions such as normalization and non-negativeness.
- 2 It is effective when one know the PSF but know little about the additive noise in the image.
- 3 Implemented in MATLAB [®]: [deconvlucy](#)

References

-  Canales-Rodríguez E.J. et al. Deconvolution in diffusion spectrum imaging. *Neuroimage*, 50(1), 136-49 (2010)
-  Biggs, D.S., Andrews, M. Acceleration of iterative image restoration algorithms. *Appl. Opt.*, 36, 17661775 (1997)

Deconvolved DSI

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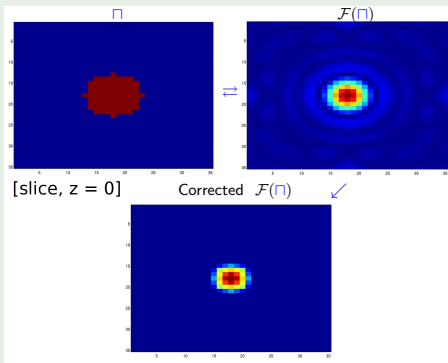
Deconvolved DSI

Description of the Reconstruction Method

Practical aspects:

In practice: $\mathcal{F}(\eta) \approx \text{FastFourierTransform}(\eta)$

Zero-padding: $35 \times 35 \times 35$ grid



ODF Computation

Description of the Reconstruction Method

Practical aspects:

- 1 The deconvolved propagator was trilinearly interpolated to a spherical lattice:
 $P(\rho, \hat{\mathbf{r}}) \equiv P(r_x, r_y, r_z)$
(50 radial points ρ along each of the 724 spatial directions $\hat{\mathbf{r}}$ in the grid).

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- 3 ODF representation in terms of real spherical harmonics using the regularization approach proposed in [Descoteaux M. et al., 2007].

$$ODF(\hat{\mathbf{r}}) \approx \sum_{l=0}^{L_{max}} \sum_{m=-l}^l o_{lm} Y_{lm}(\hat{\mathbf{r}}) \quad (L_{max} = 10 \text{ and } \lambda = 0.004)$$

References



Descoteaux M. et al. Regularized, Fast and Robust Analytical Q-Ball Imaging. *Magn Reson. Med.*, 58(3), 497-510 (2007)

ODF Maxima Extraction

Description of the Reconstruction Method

Local fiber orientations were determined as follows:

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- 2 The largest three local maxima were preserved if their amplitudes were larger than $0.4 \times ODF_{max}$, where ODF_{max} is the amplitude of the global maximum.

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- 3 All neighbors around each maximum were used to fit an ellipsoid centered at the origin. The position of the principal direction of each ellipsoid was used to specify the local fiber orientation.

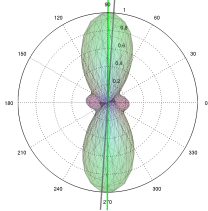
ODF Maxima Extraction

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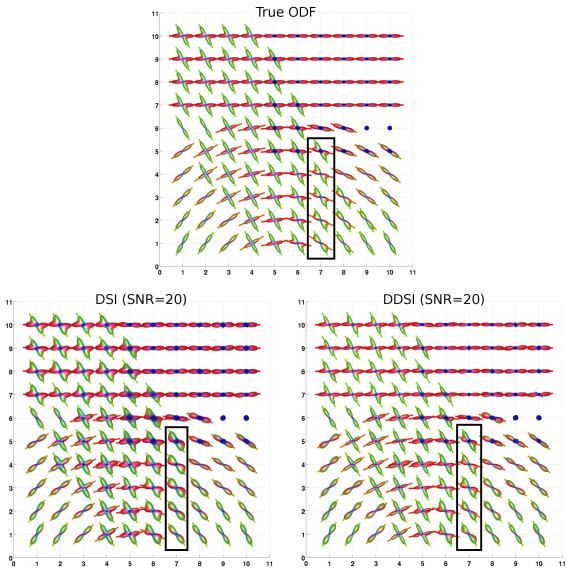
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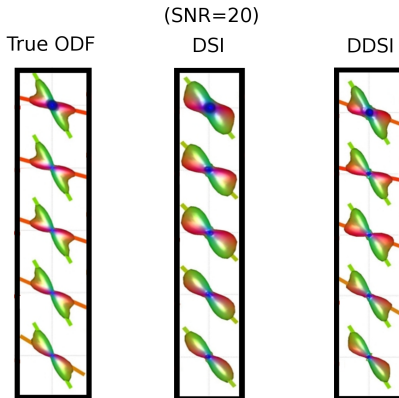
Interpolated maximum \Rightarrow \Leftarrow *Discrete maximum*



Example: 2D Synthetic Phantom

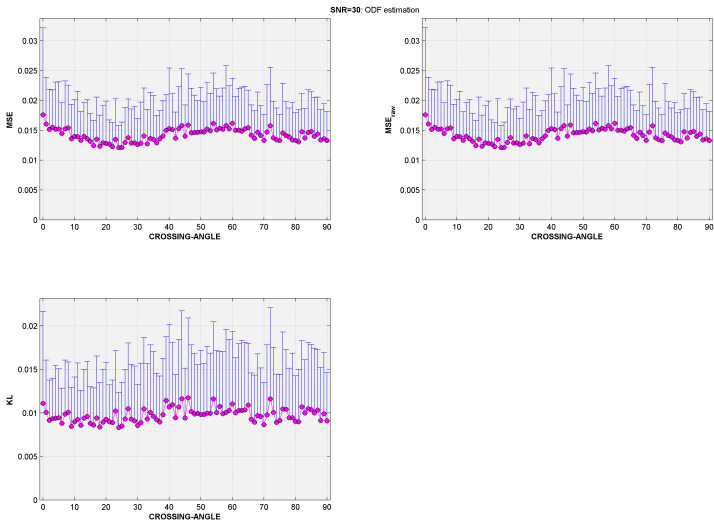


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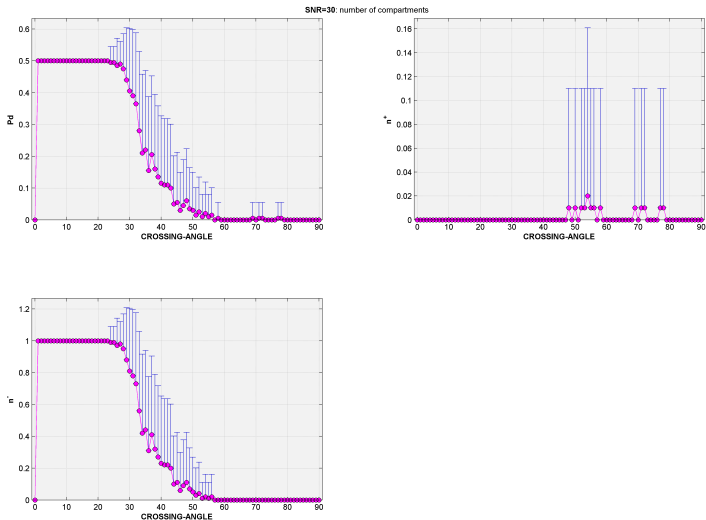
Results: Testing IV dataset

ODF estimation based metrics



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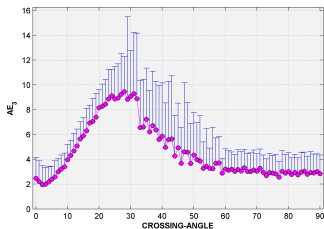
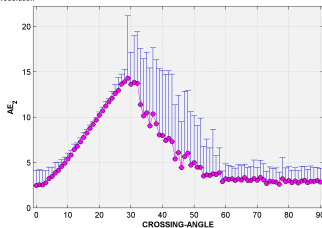
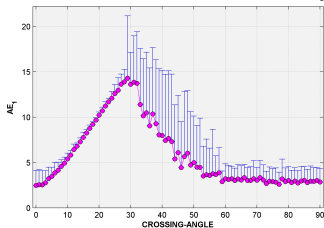
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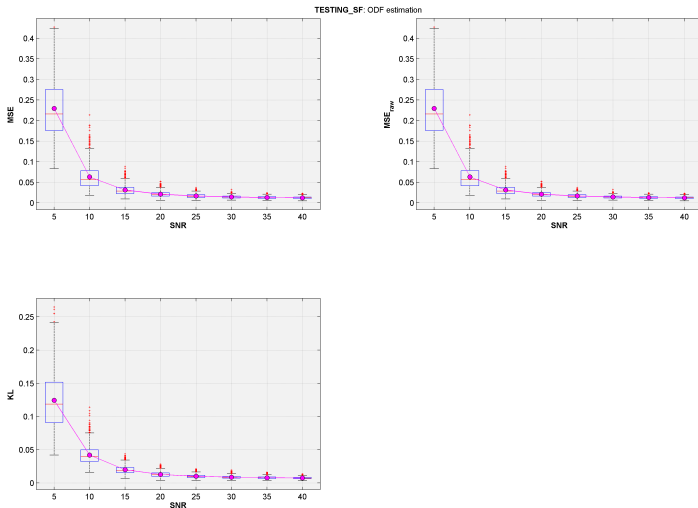
ODF estimation based metrics

SNR=30; angular resolution



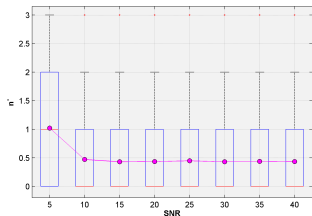
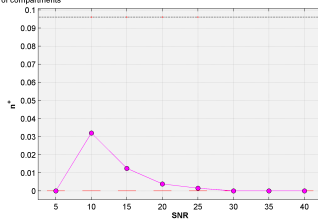
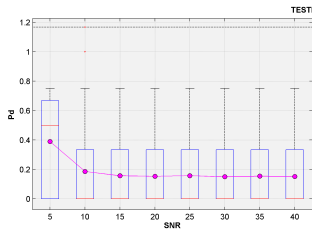
Results: Testing SF dataset

ODF estimation based metrics



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ODF estimation based metrics

